

Optical Measurement of Glucose Content of the Aqueous Humor

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Many diabetics must measure their blood glucose levels regularly to maintain good health (Appendix 1). In principle, one way of measuring the glucose concentration in the human body would be by measuring optically the glucose content of the aqueous humor in the eye. Lein Applied Diagnostics wish to assess how feasible this is,

1. purely by a system using a linear confocal scan (Appendix 2) with an LED source, as described below; and
2. by supplementing such a system with other suitable measurements.

The sensitivity of the refractive index of the aqueous humor to the glucose concentration is of the order of one part in 10^5 for a change in glucose concentration of 5mg/dl, and concentrations of between 50mg/dl and 400mg/dl need to be detected reliably.

Confocal Scanning: The use of a confocal scanning technique enables one to measure the optical depth of the aqueous humor to this required accuracy. The optical depth, D , is given by L/n where L is the physical depth of the anterior chamber and n is the refractive index of the aqueous humor. This direct measurement cannot be made in practice as the real depth of the anterior chamber changes due to corneal swelling and accommodation of the ocular lens.

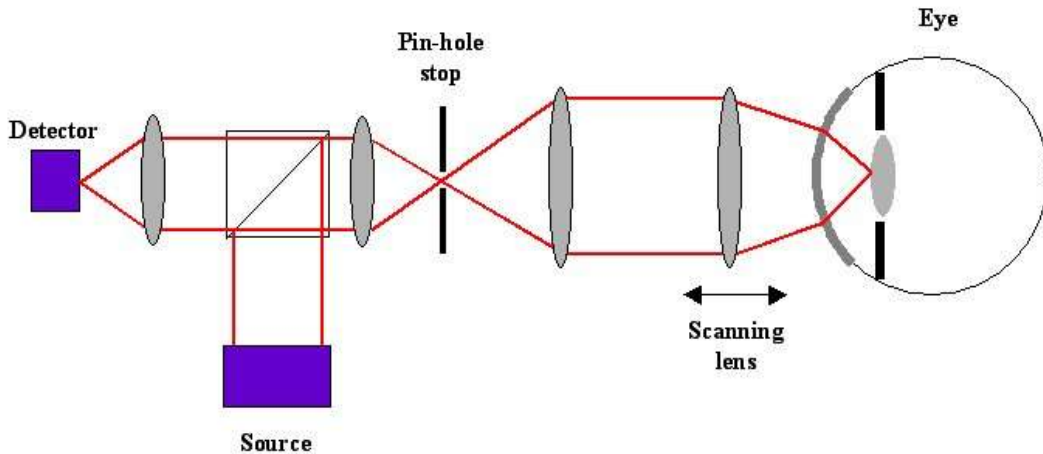
Problem 1: Is it possible to use other information obtainable from the confocal microscopy to resolve this point. In particular the measurement detects retro- reflections from the front and back of the cornea, and from the front and back of the lens, in addition to the measurements giving the location of the various surfaces. Do these retro- reflections provide the necessary information?

Problem 2: If the scan can only tell us the optical depth, what else could be measured that would enable the refractive index to be obtained to the required accuracy? In particular, can this be achieved by any of (or some combination of) the following:

1. Taking measurements at different wavelengths of light. Two wavelengths allow the measurement of the dispersion of the aqueous humor, which is a function of the glucose concentration.

in Figure 1(a)) light will be retro- reflected along its original path and will pass through the small pinhole. This light will then fall on a detector and a large intensity signal is seen. If no surface is at the focal point (as in Figure 1(b)) the reflected light diverges and hardly any makes it back through the pinhole. The detector therefore registers a low intensity signal.

This technique can be applied to the measurement of the refractive index as described below. An outline concept of a test system is shown



in Figure 2.

Figure 2. Confocal arrangement to measure the refractive index of the aqueous humor

As the scanning lens is moved backwards and forwards a bright image will be seen on the detector when the returning light reflected from the eye is focussed through the pinhole stop. At each interface (cornea/aqueous humor, aqueous humor/lens etc.) there will be light reflected such that during the scan the intensity profile shown in Figure 3 will be generated.

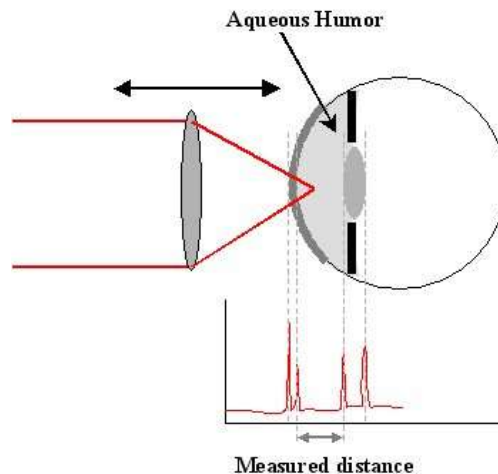


Figure 3. Intensity profile seen during the scan.

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The physical distance moved by the scanning lens between the two central intensity peaks is directly related to the refractive index of the aqueous humor. The glucose concentration can therefore be calculated by knowing the position of the scanning lens when a bright image is seen on the detector.